

A Biopolymer Transistor: Electrical Amplification by Microtubules

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ABSTRACT Microtubules (MTs) are important cytoskeletal structures engaged in a number of specific cellular activities, including vesicular traffic, cell cyto-architecture and motility, cell division, and information processing within neuronal processes. MTs have also been implicated in higher neuronal functions, including memory and the emergence of “consciousness”. How MTs handle and process electrical information, however, is heretofore unknown. Here we show new electrodynamic properties of MTs. Isolated, taxol-stabilized MTs behave as biomolecular transistors capable of amplifying electrical information. Electrical amplification by MTs can lead to the enhancement of dynamic information, and processivity in neurons can be conceptualized as an “ionic-based” transistor, which may affect, among other known functions, neuronal computational capabilities.

INTRODUCTION

MTs are long hollow cylinders made up of guanosine-triphosphate (GTP)-dependent $\alpha\beta$ -tubulin dimer assemblies (1). MTs have outer diameters of ~ 25 nm and inner diameters of 15 nm, with lengths that reach several micrometers. Recently, it has become apparent that neurons may utilize MTs in cognitive processing. MT-associated proteins, including tau and MAP2, have been implicated in such neuronal processes as learning and memory (2–4). MTs are also linked to the regulation of a number of ion channels, thus contributing to the electrical activity of excitable cells (5). Thus, MTs may play a heretofore unknown role in the processing of electrical signals within the neuron. Morphologically speaking, the elongating processes that sprout from the neuronal soma include a single axon and a variable number of dendrites; both take cable-like properties and contain abundant MTs. Dendrites, in particular, are responsible for both synaptic integration and synaptic plasticity, essential functions of neuronal activity (6,7). It is increasingly clear that cytoskeletal structures play a central role in both the process of ramification and more specialized neuronal functions, including neuronal processivity, long-term potentiation, long-term depression, and memory formation (8,9). Cytoskeletal alterations may reflect changes of neural circuits in response to learning and experience, and they must involve highly dynamic regulatory mechanisms. How this cytoskeletal control of neuronal plasticity takes form remains ill defined. Interestingly, a century ago Cajal proposed that the “cytoskeleton contain a system for the conduction of the nerve impulse” (10). To elucidate the electrodynamic properties of MTs and gain insight into the regulatory role that MTs play in dendritic

activity, we assessed whether MTs are capable of processing electrical information.

METHODS

Preparation of isolated MTs

Tubulin was polymerized with a combined GTP-taxol “hybrid” protocol, following loosely general guidelines as described in Mitchinson Lab’s online protocols (<http://mitchison.med.harvard.edu/protocols/>). Briefly, all reactions were conducted in BRB80 solution, containing 80 mM PIPES (1,4-piperazinediethanesulfonic acid), 1 mM MgCl_2 , 1 mM EGTA, and pH 6.8 with KOH. In some experiments 10 μl glycerol was added before mixing the tubulin. An aliquot of tubulin in solution (catalog No. T238, Cytoskeleton, Denver, CO) was mixed with 1 mM dithiothreitol (DTT) and 1 mM GTP in an ice bed and incubated for 5 min. Taxol (paclitaxel, Sigma; St. Louis, MO) was then added in steps, first from a 1 μM and then 10 μM solutions. Each stepwise addition of taxol was followed by incubation for 20–30 min in a water bath at 37°C. Taxol was kept in a 10-mM stock in anhydrous dimethylsulfoxide (DMSO). In some instances, the tubulin-containing solution was mixed with BRB80 solution ($\times 2$) and added 2 mM DTT, 2 mM GTP, and 20% DMSO, followed by incubation at 37°C for 20–30 min. Polymerized tubulin was centrifuged in a microfuge for 30 min at 14,000 rpm. Two-thirds of the supernatant was discarded, and the remainder constituted the MT sample, which was further stabilized by addition of 1 mM GTP and 1 μM taxol. MTs were visualized under phase contrast microscopy (IMT-2, Olympus, Tokyo, Japan; $\times 60$) to ascertain the lack of nucleated centers induced by higher concentrations of taxol. MTs were stable at room temperature for up to 2 days.

Measurement of electrical signals in isolated MTs

Electrical data were collected with a modified dual “patch-clamp” setup as previously reported (11). Briefly, the electrical setup consisted of two independent patch-clamp amplifiers, PC501 and PC501A (Warner Instruments, Hamden, CT), with 1-G Ω and 10-G Ω feedback resistors, respectively, one to stimulate the isolated MT (stimulus, s) and the other to collect current signals (collection, c). Electrical signals were simultaneously collected by respective analog inputs of an analog-to-digital (A/D) converter (TL-1 DMA Interface, Axon Instruments, Foster City, CA). Voltage stimulus protocols were constructed in Clampex 5.5.1 (Axon Instruments) run from a computer. The sampling intervals varied depending on the protocol, such that in most cases a 100-ms signal length contained at least 400 samples. Offset tip potentials within the range of a few millivolts were

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compensated immediately before data acquisition. Further zeroing of the offset signal was conducted offline during data processing. Signals were Gaussian filtered at a cutoff frequency of 2.2 kHz. Pipettes were made from borosilicate capillaries (1.2-mm external diameter) and were pulled with tip diameters below $3\ \mu\text{m}$. The pipettes contained and were immersed in a solution containing in mM: 135 KCl, 5 NaCl, 0.8 MgCl_2 , 1.2 CaCl_2 , 10 Hepes. Occasionally, the pipette tip contained a 1:10 dilution of the taxol solution to help attach the MT. The pipettes were connected to the electrodes and head stage of their respective patch-clamp amplifiers. Agar bridges containing 3% agar in 150 mM KCl solution grounded both amplifiers to the chamber. The circuit was closed by two AgCl-plated Ag ground electrodes in solutions far away (1–2 cm) from the pipette tips.

Data analysis

Data were acquired at 2 KHz and further filtered offline for display and analysis when required. Noise analysis was conducted as Lorentzian spectral analysis with a subroutine of Axograph 4.0 (Axon Instruments) from unfiltered files where the variance versus frequency was plotted for paired experiments before and after MT attachment was obtained in the experiment. The method for deriving the amplification is different for the square pulse and for the triangle wave. In the case of the square pulse, we evaluated the average amplitude in solution only and with MT attached for the same conditions. The amplification is simply the ratio. In the case of triangle pulses, a different strategy was used, using the slope of the linear regression of the MT-attached data as a function of the solution-only data at the pulse times. Data are expressed as $n = \text{number of files averaged} \pm \text{SE}$, where t -test was used to assess statistical significance at $p < 0.05$.

RESULTS

MTs were formed and stabilized as indicated in Methods. Isolated MTs were visualized and identified under phase contrast microscopy and connected to the tips of two patch-clamp amplifiers (Fig. 1 *a*), such that electrical stimulation could be applied to one of them, whereas the elicited signal could be collected with the other one (Fig. 1 *b*). MTs were electrically stimulated by applying 5–10-ms input voltage pulses with amplitudes in the range of $\pm 200\ \text{mV}$. The resulting electrical signals were obtained at the opposite end of an MT, 20–50 μm away with a pipette also connected to a patch amplifier, which was kept “floating” at 0 mV. We observed two remarkable findings. First, coupling of the stimulus pipette to an MT increased the overall conductance of the pipette by $>300\%$. The stimulus pipette resistance in KCl saline (135 mM) was $21.6 \pm 0.6\ \text{M}\Omega$ ($n = 16$). The coupling ratio between pipettes in solution was $41\% \pm 12\%$ before attachment to an MT. Thus, the collection pipette “read” $\sim 40\%$ of the stimulus in solution. The evoked current increased from $1.91 \pm 0.13\ \text{nA}$ ($n = 16$) to $2.78 \pm 0.17\ \text{nA}$ ($n = 35$) after attachment (Fig. 2 *a*). The signals reaching the collection site were in 30/35 of the cases higher than those obtained in free solution, indicating that the MT amplified both the electrical pulse injected at the stimulus site and the collection site as well (Fig. 2 *a*). Transfer amplification ratios were up to 2.35 with an average of 1.69 ± 0.06 ($n = 30$, Fig. 2 *c*). Thus, MTs improve electrical connectivity between two locations in saline solution. The currents measured at the collection site were linearly de-

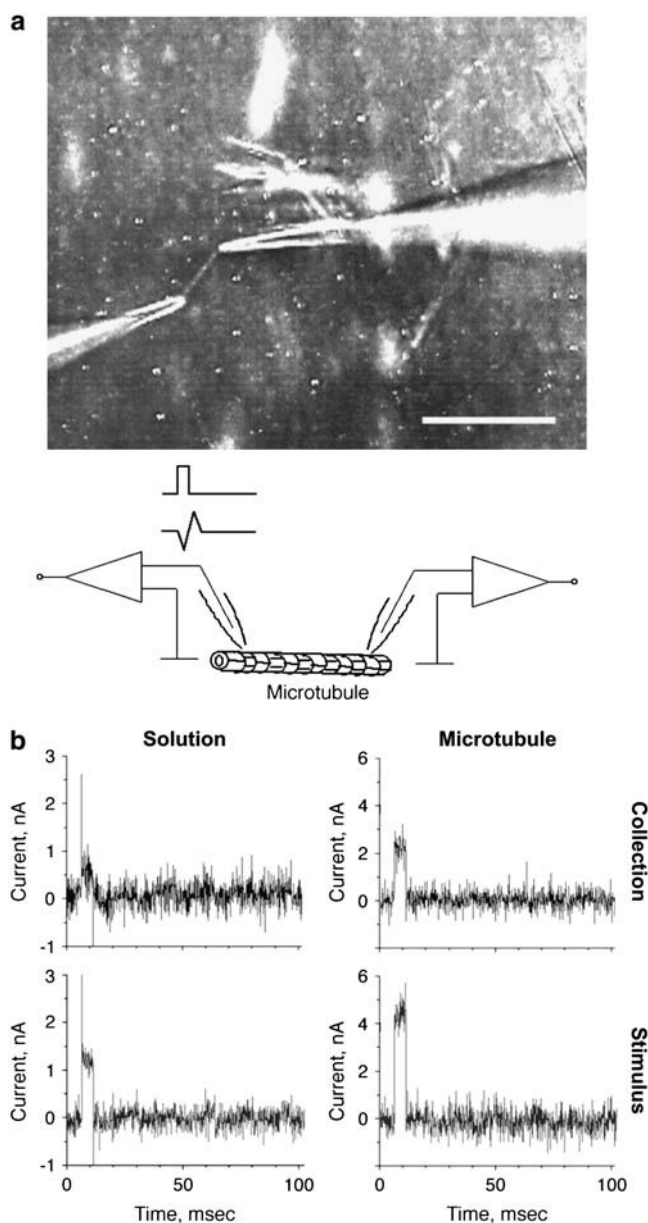


FIGURE 1 Electrical setup. (*a*) (*Top*) A free-floating MT was “connected” to two patch pipettes. Horizontal bar is $50\ \mu\text{m}$. (*Bottom*) Electrical signals were applied to one end and collected from the other end with two patch-clamp amplifiers. (*b*) Voltage pulse ($+100\ \text{mV}$) was first applied to the “stimulus” pipette in saline solution. The recorded current from stimulus pipette (*left bottom*) and electrical coupling by the “collection” pipette (*left top*) were obtained. A similar approach was repeated after MT attachment. Currents were higher after attachment to an MT (*right*), compared to saline solution (*left*). Representative tracings from 16 experiments are shown.

pendent on the stimulus pipette input voltage, indicating a strictly inverse ohmic response, i.e., linear amplification (Fig. 2 *b*). The MT conductances reached up to 9 nS, much higher than that expected from channel conductances (5–200 pS, Fig. 2 *b*, *inset*). The electrical amplifying effect of the MT was observed in either direction (stimulus by either

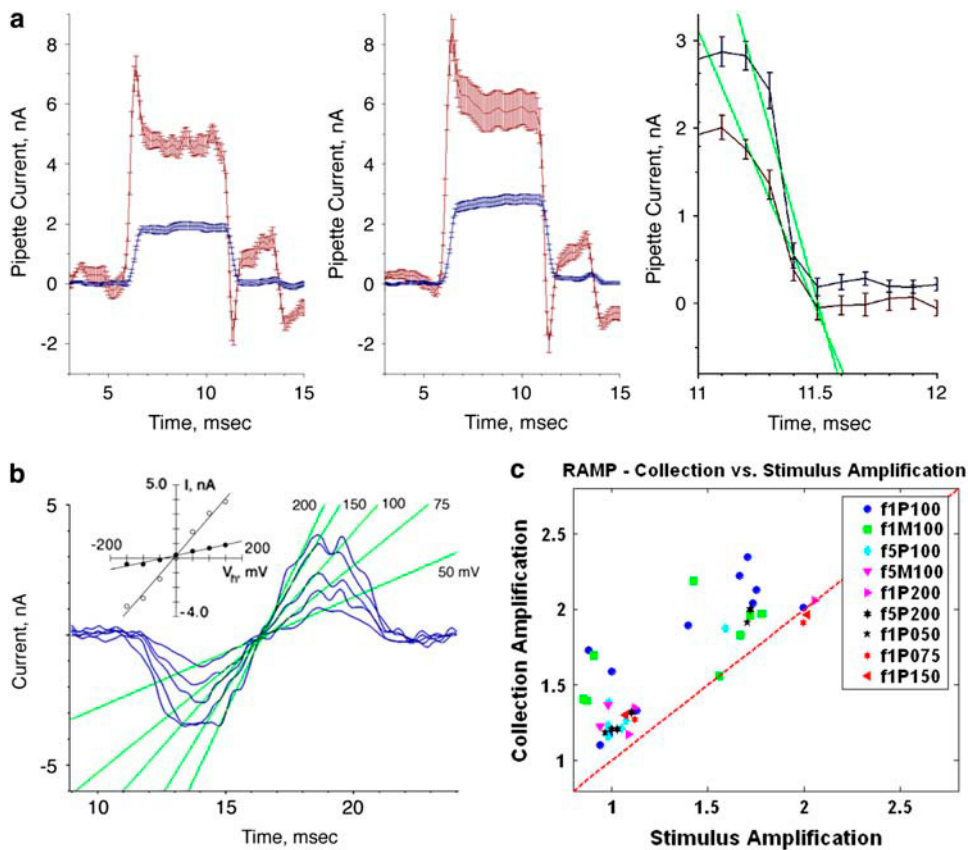


FIGURE 2 Pulse stimulation of isolated MTs. (a) Average electric pulses (100 mV, 5 ms) for the “stimulus” (red) and the “collection” (blue) sites. Data on the left indicate the signal before attachment. Values are the mean \pm SE for five pipettes with similar electrical properties. The decay response of the MT-connected tip at the end of the electrical pulse was $\sim 40 \mu\text{s}$ faster after connection (right). (b) MT-attached signals on the collection site for 5-ms ramps at different voltages. Fitted linear slopes (green) indicate a linear response. (Inset) Current-to-voltage relationship for a connected MT (open circles) compared to free solution (solid circles). The conductance is linear. The signals increased in average by 1.69 at an average distance of $35 \mu\text{m}$. (c) Correlation of amplification ratios between the stimulus and collection sites. Identity line (red) indicates no amplification by the connected MT. Amplification factors are shown for either 10 ms (f1) or 5 ms (f5) ramps for positive (P) and negative (M) potentials (last three digits).

amplifier). To further prove the linear response in amplification as well as the speed of the electrical amplifying phenomenon, voltage ramps were also applied within the range of ± 100 mV at two different rates (100 V/s and 20 V/s, Fig. 2 b). The stimulated currents at either rate were again linear, showing a remarkable reproducibility within the range of voltages studied. The amplification ratio remained constant within the range of voltages and rates tested, and the noise in the signal was, as expected, increased as well. The fastest ramps tested showed, however, a $40\text{-}\mu\text{s}$ (or shorter) delay between the stimulus and collection sites, which was consistent with the shift in voltage decay after pulse stimulation (Fig. 2 a, right). This suggests a lower bound for the transfer rate of the electrical signal of the order of 1.0 m/s. In two out of seven experiments, electrical amplification further increased by addition of GTP (1 mM) to the bath solution (data not shown).

DISCUSSION

Our findings demonstrate that electrical amplification by MTs is equivalent to the polymer's ability to act as a biomolecular transistor at its core. Based on a minimalistic model, both a constant electrical polarization and an active component are required. Despite current interest and extensive literature on the properties and functions of MTs,

practically nothing is known about the ionic properties of the MTs intrapolymeric compartment. However, molecular dynamics simulation of tubulin structure (12,13) indicates a strong negative surface charge distribution of the order of $20e^-$ per monomer, distributed more on the outer surface than in the inner core with ratio of $\sim 2:1$. Our findings support these theoretical results manifested in the model via a constant (permanent) electric polarization, which follows localized Nernst potentials arising from asymmetries in the ionic distributions between the intra- and extra-MT environments. This polarization is modulated by electrical stimulation such that the forward-reverse biased junctions of an intramolecular transistor (Fig. 3) creates a proper MT-adjacent ionic cloud environment, which allows amplification of axially transferred signals. The proposed model implies that intrinsic semiconductive like properties of the structured tubulin dimers are such that an effective transistor is being formed (14) whose gating ability to modulate localized charges may help amplify axial ionic movements. Recent studies aimed at solving the Poisson-Boltzmann equation for a section of an MT in ionic conditions similar to those reported here (i.e., 150 mM saline) (12) suggest a highly ordered charge distribution. Positive charges are “sandwiched” within a two-layered structure of negative charges facing either side of the MT. There also is an asymmetrical distribution of charges on the plus-minus

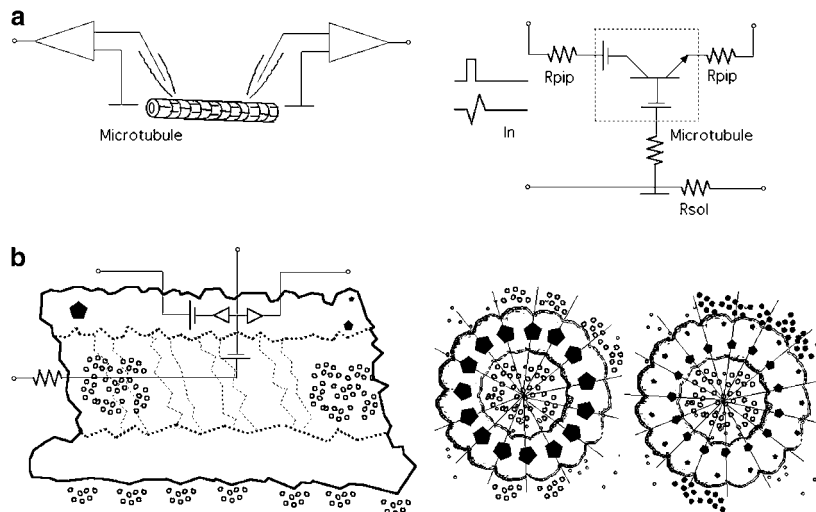


FIGURE 3 Electrical model of the MT. (a) Effective electrical model of the MT (right) is consistent with an electrical amplifier, including a molecular “biotransistor” and energy sources in the form of batteries to polarizing the amplifier. (b) Relation of electrical model to the electrostatic properties of an MT for both the plus and minus ends, potential isocontours, reproduced from Baker et al. (11). Electrostatic profile of a cross section of the MT (right) shows periodic distribution of positive charges (black) on the surface of the electronegative MT. Periodically distributed charges (large and small pentagons) maintain a “band junction” in the surrounding counterions. This is based on an electric potential difference in the MT wall (open circles and solid circles for cations and anions, respectively).

orientation of the MT. However, to better understand the dynamical properties of the electric field around the MT, it is imperative to apply a method that incorporates the diffusive part of the system. A possible candidate is the Poisson-Nernst-Planck (PNP) theory in which both the electrical potential generated by fixed charges and the flux generated by the moving charges due to potential and concentration gradients are taken into account. This method has been applied successfully to describe ion channels (15), and it would be interesting to test the applicability of this method to a system as large as the MT.

An electrical amplifier by a cytoskeletal biopolymer such as the MT provides a relevant and important key component to an electrodynamic network in conjunction with electrical coupling by current generators (i.e., MT-regulated channels (5)) and MT-coupled intracellular transmission lines (F-actin) (11,16). It is therefore plausible that electrical amplification by MTs may play an important role in processing electrical information in neuronal function. Our data further indicate that this phenomenon is accomplished with speed at least as high as those reported for cable properties in neurites (17).

MT networks (MTNs) play relevant roles in neuron formation and function (18–20). Interconnected bundles of MTs, for example, are present in the axon, the axon hillock, and the dendritic shaft, all regions where ion channels are found. In particular, dendritic MTs are arranged in grid-like networks of mixed polarity interconnected by MAP2s. Thus, we envision a mechanism in which MT-ion channel interactions may regulate synaptic plasticity by the MT’s ability to allow spatially oriented intracellular electrical signals in connection with actin filaments also able to transmit electrical information (11,16). According to this hypothesis, postsynaptic electrical signals elicit ion waves along the associated actin filaments at the synaptic spine that propagate to the MTN, where they serve as input signals. The MTN, operating as a large high dimensional “state

machine”, evolves these input states, e.g., by supporting nonlinear wave collisions. The output from the MTN is the state of the system that is being “read” (sensed) to propagate and electrically stimulate remote voltage-sensitive ion channels. Thus, our findings provide several advantages in the context of neural function. Cable theory analysis of dendrites (21,22) has challenged the simple integrate and fire models, suggesting that dendrites impose a heavy conductance load on the soma, acting as low-pass filters of postsynaptic potentials, hence changing the response to synaptic activities (22). The dendritic electrical properties are dynamically changed by modulation of voltage-gated ion channels (6,22,23) and by changes in cytoskeletal structures (25–27). Thus, MT electrical amplification may be central to revised models of neuronal adaptability (23,28,29) providing renewed support to nonlinear models of neuronal activity.

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REFERENCES

1. Dustin, P. 1984. Microtubules. Springer-Verlag, Berlin.
2. Khuchua, Z., D. F. Wozniak, M. E. Bardgett, Z. Yue, M. McDonald, J. Boero, R. E. Hartman, H. Sims, and A. W. Strauss. 2003. Deletion of the N-terminus of murine MAP2 by gene targeting disrupts hippocampal CA1 neuron architecture and alters contextual memory. *Neuroscience*. 119:101–111.
3. Wong, R. W., M. Setou, J. Teng, Y. Takei, and N. Hirokawa. 2002. Overexpression of motor protein KIF17 enhances spatial and working memory in transgenic mice. *Proc. Natl. Acad. Sci. USA*. 99: 14500–14505.
4. Woolf, N. J., M. D. Zimmerman, and G. V. W. Johnson. 1999. Hippocampal microtubule-associated protein-2 alterations with contextual memory. *Brain Res*. 821:241–249.

5. Johnson, B. D., and L. Byerly. 1994. Ca^{2+} channel Ca^{2+} -dependent inactivation in a mammalian central neuron involves the cytoskeleton. *Pflügers Arch.* 429:14–21.
6. Johnston, D., J. C. Magee, C. M. Colbert, and B. R. Christie. 1996. Active properties of neuronal dendrites. *Annu. Rev. Neurosci.* 19:165–186.
7. Ramon-Moliner, E. 1968. The morphology of dendrites. In *The Structure and Function of Nervous Tissue*. G. H. Bourne, editor. Academic Press, New York. 205–267.
8. Abel, T., and K. M. Lattal. 2001. Molecular mechanisms of memory acquisition, consolidation and retrieval. *Curr. Opin. Neurobiol.* 11: 180–187.
9. Bliss, T. P., and G. A. Collingridge. 1993. Synaptic model of memory: long-term potentiation in the hippocampus. *Nature.* 361:31–39.
10. Azmitia, E. C. 2002. Cajal's hypotheses on neurobionics and neurotropic factor match properties of microtubules and S-100 beta. *Prog. Brain Res.* 136:87–100.
11. Lin, E., and H. F. Cantiello. 1993. A novel method to study the electrodynamic behavior of actin filaments. Evidence for cable-like properties of actin. *Biophys. J.* 65:1371–1378.
12. Baker, N. A., D. Sept, S. Joseph, M. J. Holst, and J. A. McCammon. 2001. Electrostatics of nanosystems: application to microtubules and the ribosome. *Proc. Natl. Acad. Sci. USA.* 98:10037–10041.
13. Tuszynski, J. A., J. A. Brown, E. Crawford, E. J. Carpenter, M. L. A. Nip, J. M. Dixon, and M. V. Sataric. 2005. Molecular dynamics simulations of tubulin structure and calculations of electrostatic properties of microtubules. *Math. Comput. Model.* 41:1055–1070.
14. Azaroff, L. V., and J. J. Brophy. 1963. In *Electronic Processes in Materials*. McGraw-Hill Book Co., Inc., New York. 268–304.
15. Eisenberg, R. S. 1996. Computing the field in proteins and channels. *J. Membr. Biol.* 150:1–25.
16. Tuszynski, J. A., S. Portet, J. M. Dixon, C. Luxford, and H. F. Cantiello. 2004. Ionic wave propagation along actin filaments. *Biophys. J.* 86:1890–1903.
17. Fromherz, P., and C. O. Müller. 1994. Cable properties of a straight neurite of a leech neuron probed by a voltage-sensitive dye. *Proc. Natl. Acad. Sci. USA.* 91:4604–4608.
18. Dehmelt, L., and S. Halpain. 2004. Actin and microtubules in neurite initiation: are MAPs the missing link? *J. Neurobiol.* 58:18–33.
19. Dent, E. W., and K. Kalil. 2001. Axon branching requires interactions between dynamic microtubules and actin filaments. *J. Neurosci.* 21: 9757–9769.
20. Yamada, K. M., B. S. Spooner, and N. K. Wessells. 1970. Axon growth: roles of microfilaments and microtubules. *Proc. Natl. Acad. Sci. USA.* 66:1206–1212.
21. Hodgkin, A. L., and A. F. Huxley. 1952. A quantitative description of membrane current and its application to conduction and excitation in nerve. *J. Physiol.* 117:500–544.
22. Rall, W., and J. Rinzel. 1973. Branch input resistance and steady attenuation for input to one branch of a dendritic neural model. *Biophys. J.* 13:648–688.
23. Koch, C., and I. Segev. 2000. The role of single neurons in information processing. *Nat. Neurosci.* 3:1171–1177.
24. Schiller, J., and Y. Schiller. 2001. NMDA receptor-mediated dendritic spikes and coincident signal amplification. *Curr. Opin. Neurobiol.* 11:343–348.
25. Kaech, S., H. Parmar, M. Roelandse, C. Bornmann, and A. Matus. 2001. Cytoskeletal microdifferentiation: a mechanism for organizing morphological plasticity in dendrites. *Proc. Natl. Acad. Sci. USA.* 98:7086–7092.
26. Scott, E. K., and L. Luo. 2001. How do dendrites take their shape? *Nat. Neurosci.* 4:359–365.
27. Vetter, P., A. Roth, and M. Häusser. 2001. Propagation of action potentials in dendrites depends on dendritic morphology. *J. Neurophysiol.* 85:926–937.
28. Mel, B. W. 1999. Why have dendrites? A computational perspective. In *Dendrites*. G. N. Stuart, N. Spruston, and M. Häusser, editors. Oxford University Press, Oxford. 271–289.
29. Segev, I., and M. London. 2000. Untangling dendrites with quantitative models. *Science.* 290:744–750.